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**ELECTRODE ARRAY WITH NON-UNIFORM
ELECTRODE SPACING**

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Technical Field

Background Art

10 The array is connected to a receiver-stimulator unit, which in turn typically communicates transcutaneously with an externally worn speech processor and sound transducer.

All commercially available cochlear implants utilise electrode arrays in which the electrodes are substantially equally spaced along the length of the array.

It is an object of the present invention to provide an electrode array which improves the fidelity of the reproduction of the audio spectrum in the percent of the audible imple...

According to one aspect, the present invention provides an
5 intracochlear electrode array in which the electrodes are closer together at the
apical end of the array. This may be achieved in various ways – for example,
★ || by a uniformly graduated change in spacing, or by selecting two or more
regions of the electrode array to have different spacings.

According to another aspect, the present invention provides an electrode array with the spacing of electrodes varied so as to provide a higher density of electrodes at specific regions – for example, along a part of the array intended to stimulate one or more regions of the neural structures corresponding to frequency bands which are considered particularly important for speech recognition. This could be based on many different considerations – the essence of this aspect of the invention is simply to provide electrodes at reduced spacing in areas of particular interest.

Brief Description of the Drawings

The invention will now be described with reference to the accompanying figures, in which:

Figure 1 is a schematic illustration of a conventional electrode array in a scala tympani; and

Figure 2 is a schematic illustration of an electrode array with non-uniform spacing of electrodes.

Referring to figure 1, this is based upon an X-Ray of an implanted device having a curved configuration, for example an array according to PCT/AU99/00391 by Cochlear Limited. It will be appreciated that this is a sectional view showing the scala tympani 10, which in fact curves into the page, but for present purposes the invention can be explained with reference to a two dimensioned projection.

Dotted line 15 represents the organ of Corti, on which the audio
15 receptors 12 are disposed at the intersection of radial lines 11 (only one thus
labeled) and the organ of Corti 15. Radial lines 11 are shown extending from
the modiolar centre 16, and are of course, purely represented for the purpose
of illustrating the present inventive concept. Receptors 12 are composed of
neural structures, including spiral ganglion cells, which extend radially inward
20 from the organ of Corti 15. It is in fact these cells which are stimulated by the
stimuli produced by electrodes in a cochlear implant.

It will be noted that receptors 12 are disposed at equal intervals along the organ of Corti 15 (at critical bands), even as the curvature increases as the cochlea spirals inwards. The most effective stimulation of these receptors is achieved by direct stimulation by electrodes, and so cochlear implants have been traditionally constructed with electrodes spaced equally to correspond with the spacing of these critical bands. These electrodes are shown as elements 13 on cochlear implant 14.

It has been determined that receptors are more sensitive on the inner wall 18 of the scala tympani 10. Accordingly, it has been found that a better result is achieved by a cochlear implant having electrodes stimulating receptors on the inner wall. To achieve this, the electrodes are caused to lie

against the inner wall 18, to make contact with receptors 17 (lying on the intersection of radial lines 11 and the inner wall 18 of scala timpani 10).

As can be seen in figure 2, the receptors 17 on the inner wall 18, are spaced more and more closely together, as they approach the centre of the spiral of the cochlea. Thus, to maintain effective stimulation contact with receptors 17, electrodes 13 of the electrode array 14 are spaced with decreasing separation to each other the closer they approach the apical end of the electrode array 14.

Therefore, with an understanding of the physiology and geometry of the cochlea together with an understanding of the tonotopical nature of the cochlea, an electrode array can be designed to improve the fidelity of the reproduction of the audio spectrum in the percept of the cochlear implant recipient. This can be done by arranging the placement of the electrodes along the electrode array such that the spectral coverage of the electrodes are maximised to ensure optimum stimulation of the cochlea is achieved.

It will be appreciated that in the application of the present invention, the excitation by the electrodes is assumed to be substantially radial.

It may also be desired to take into account two further effects. The structures are considerably more complex than is apparent from the schematics. At the basal end of the scala tympani, the organ of Corti lies closer to the inner wall 18 and the spacing of the most basal electrodes could be reduced to take account of this. At the apical end, there is a greater angular offset between the organ of Corti 15 and the underlying cell bodies, and again the spacing could be adjusted to account for this effect.

25 It will be appreciated by those skilled in the art that the present invention can be readily manufactured by existing techniques, and could be of any desired electrode geometry or cross-sectional shape. The present invention is concerned with the spacing of the electrodes, not their construction.